The 5th annual Symposium on Data Science and Statistics **CS20 - Neural Network Analysis**

A Novel Network Architecture Combining Central-Peripheral Deviation with CNNs for DTI Studies

Soyun Park, University at Buffalo June 9, 2022



- Introduction
- II. Methods
 - ✓ Concept of CPD
 - ✓ CNN+MLP architecture
- III. Results
 - ✓ Applications to DTI studies: MagNeTS, ICBM
- IV. Discussion

Contents

Introduction

- II. Methods
 - ✓ Concept of CPD
 - ✓ CNN+MLP architecture
- III. Results
- ✓ Applications to DTI studies: MagNeTS, ICBM IV. Discussion

Contents



Geography?

- Pittsburgh vs. Seoul
 - Shape
 - Structure



Pittsburgh, Pennsylvania, USA (Credit: Google Maps)



Seoul, South Korea

• Geography?

- Pittsburgh vs. Seoul
 - Shape
 - Structure

Classification



Pittsburgh, Pennsylvania, USA (Credit: Google Maps)



Seoul, South Korea

- DTI studies white matter of the brain
- Diffusion-Weighted Imaging (DWI) shows water movement lacksquarealong the tissues and models the difference of signals between baseline image and DWI image at b-value (i.e., b=1000)

$$\ln\left(\frac{S}{S_0}\right) = -\gamma^2 G^2 \delta^2 (\Delta - \delta/3) D = -\frac{1}{2} \delta^2 (\Delta - \delta/3) D = -\frac$$

 The diffusion tensor D is used to measure the degree of anisotropy and structural orientation that characterizes DTI



Credit: imagilys.com

-bD



- DTI studies white matter of the brain
- Diffusion-Weighted Imaging (DWI) shows water movement lacksquarealong the tissues and models the difference of signals between baseline image and DWI image at b-value (i.e., b=1000)

$$\ln\left(\frac{S}{S_0}\right) = -\gamma^2 G^2 \delta^2 (\Delta - \delta/3) D = -$$

 The diffusion tensor D is used to measure the degree of anisotropy and structural orientation that characterizes DTI



Credit: imagilys.com

-bD



- DTI studies white matter of the brain
- Diffusion-Weighted Imaging (DWI) shows water movement lacksquarealong the tissues and models the difference of signals between baseline image and DWI image at b-value (i.e., b = 1000

$$\ln\left(\frac{S}{S_0}\right) = -\gamma^2 G^2 \delta^2 (\Delta - \delta/3)D = -$$

• The diffusion tensor D is used to measure the degree of anisotropy and structural orientation that characterizes DTI



Credit: imagilys.com

-bD



- DTI studies white matter of the brain
- Diffusion-Weighted Imaging (DWI) shows water movement along the tissues and models the difference of signals between baseline image and DWI image at b-value (i.e., b=1000)

$$\ln\left(\frac{S}{S_0}\right) = -\gamma^2 G^2 \delta^2 (\Delta - \delta/3)D = -$$

• The diffusion tensor D is used to measure the degree of anisotropy and structural orientation that characterizes DTI



Credit: imagilys.com

-bD



- DTI studies white matter of the brain
- Diffusion-Weighted Imaging (DWI) shows water movement along the tissues and models the difference of signals between baseline image and DWI image at b-value (i.e., b=1000)

$$\ln\left(\frac{S}{S_0}\right) = -\gamma^2 G^2 \delta^2 (\Delta - \delta/3)D = -$$

 The diffusion tensor D is used to measure the degree of anisotropy and structural orientation that characterizes DTI



Credit: imagilys.com





- Both normal subjects and patients with brain tumors, Alzheimer's, schizophrenia, etc.
- ROI Analysis, Voxel-Based Analysis, Tract-Based Spatial Statistics (e.g., tractography)
- Manual annotation of region by experts

Existing DTI studies



Credit: Jbabdi and Johansen-Berg 2011





• An important issue was not addressed in DTI studies.



An important issue was not addressed in DTI studies. Can we define a measure that distinguishes different groups?



- An important issue was not addressed in DTI studies.
 Can we define a measure that distinguishes different groups?
- Assumption: If we find a measure that defines some good feature in DTI, then we don't have to depend on previous regions of interest (ROI) that requires manual feature selection.



- An important issue was not addressed in DTI studies. Can we define a measure that distinguishes different groups?
- Assumption: If we find a measure that defines some good feature in DTI, then we don't have to depend on previous regions of interest (ROI) that requires manual feature selection.

Holistic approach to brain images searching for patterns

- Introduction Ι.
- II. Methods
 - ✓ Concept of CPD
 - ✓ CNN+MLP architecture
- III. Results
- ✓ Applications to DTI studies: MagNeTS, ICBM IV. Discussion

Contents

Mathematics of DTI

- Diffusion process by an ellipsoid (Basser et al., 1994)
- Diffusion Tensor A symmetric 3x3 matrix for each voxel
- Shape and orientation eigenvalues and corresponding eigenvectors

$$D = \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{xy} & D_{yy} & D_{yz} \\ D_{xz} & D_{yz} & D_{zz} \end{bmatrix} = \begin{bmatrix} \mathbf{v}_1 \\ \mathbf{v}_2 \\ \mathbf{v}_3 \end{bmatrix} \begin{bmatrix} \lambda_1 & 0 & 0 \\ 0 & \lambda_2 & 0 \\ 0 & 0 & \lambda_3 \end{bmatrix} \begin{bmatrix} \mathbf{v}_1 & \mathbf{v}_2 & \mathbf{v}_3 \end{bmatrix}$$



Fig. 5.2 A diffusion ellipsoid can be fully characterized from diffusion measurements along six independent axes.



Mathematics of DTI

- Diffusion process by an ellipsoid (Basser et al., 1994)
- Diffusion Tensor A symmetric 3x3 matrix for each voxel
- Shape and orientation eigenvalues and corresponding eigenvectors

$$D = \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{xy} & D_{yy} & D_{yz} \\ D_{xz} & D_{yz} & D_{zz} \end{bmatrix} = \begin{bmatrix} \mathbf{v}_1 \\ \mathbf{v}_2 \\ \mathbf{v}_3 \end{bmatrix} \begin{bmatrix} \lambda_1 & 0 & 0 \\ 0 & \lambda_2 & 0 \\ 0 & 0 & \lambda_3 \end{bmatrix} \begin{bmatrix} \mathbf{v}_1 & \mathbf{v}_2 & \mathbf{v}_3 \end{bmatrix}$$

$$FA = \frac{1}{\sqrt{2}} \frac{\sqrt{(\lambda_1 - \bar{\lambda})^2 + (\lambda_2 - \bar{\lambda})^2 + (\lambda_3)^2}}{\sqrt{\lambda_1^2 + \lambda_2^2 + \lambda_3^2}}$$

where $\bar{\lambda} = \frac{\lambda_1 + \lambda_2 + \lambda_3}{3} = MI$



Fig. 5.2 A diffusion ellipsoid can be fully characterized from diffusion measurements along six independent axes.

Mathematics of DTI

- Diffusion process by an ellipsoid (Basser et al., 1994)
- Diffusion Tensor A symmetric 3x3 matrix for each voxel
- Shape and orientation eigenvalues and corresponding eigenvectors

$$D = \begin{bmatrix} D_{xx} & D_{xy} & D_{xz} \\ D_{xy} & D_{yy} & D_{yz} \\ D_{xz} & D_{yz} & D_{zz} \end{bmatrix} = \begin{bmatrix} \mathbf{v}_1 \\ \mathbf{v}_2 \\ \mathbf{v}_3 \end{bmatrix} \begin{bmatrix} \lambda_1 & 0 & 0 \\ 0 & \lambda_2 & 0 \\ 0 & 0 & \lambda_3 \end{bmatrix} \begin{bmatrix} \mathbf{v}_1 & \mathbf{v}_2 & \mathbf{v}_3 \end{bmatrix}$$

$$FA = \frac{1}{\sqrt{2}} \frac{\sqrt{(\lambda_1 - \bar{\lambda})^2 + (\lambda_2 - \bar{\lambda})^2 + (\lambda_3 - \bar{\lambda})^2}}{\sqrt{\lambda_1^2 + \lambda_2^2 + \lambda_3^2}}$$

where $\bar{\lambda} = \frac{\lambda_1 + \lambda_2 + \lambda_3}{3} = MI$

Ideas for a new measure

Ideas for a new measure

1. Semi-variogram (Matheron, 1963)

$$\gamma(h) = \frac{1}{2V} \iint \int \int \int_{V} [f(M+h) - f(M)]^2 dx$$

dV

Ideas for a new measure

1. Semi-variogram (Matheron, 1963)

$$\gamma(h) = \frac{1}{2V} \iint \int \int \int_{V} [f(M+h) - f(M)]^2 dx$$

2. Polycentric Circle Pooling (Qi et al., 2020)

dV

Fig. 3. Example of the pooling strategy in PCP with four-channel maps of size 16×16 and five circle centers. The annular subregions are shown in different colors, except for the dark gray indicating the exclusive cells.

Young at z=38

Senior at z=38

Young at z=38

Senior at z=38

Young at z=38

Senior at z=38

Young at z=38

Senior at z=38

•
$$CPD = \mu_2 - (\mu_1 - \mu_2) = 2\mu_2 - \mu_1$$

• $sCPD = \frac{\mu_2 - (\mu_1 - \mu_2)}{\sqrt{\varphi}} = \frac{2\mu_2 - \mu_1}{\sqrt{\varphi}}$

where
$$\mu_i = \frac{\int_{R_i} f(r,\theta) dA}{\int_{R_i} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_i} f(r,\theta) r dr d\theta}{\int_0^{2\pi} \int_0^{r_i} 1_{f(r,\theta)} r dr d\theta}, \quad \varphi = \frac{\int_{R_1} \{f(r,\theta) - \mu_1\}^2 dA}{\int_{R_1} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_1} \{f(r,\theta) - \mu_1\}^2 r dr d\theta}{\int_0^{2\pi} \int_0^{r_1} 1_{f(r,\theta)} r dr d\theta}, \quad i = 1, 2,$$

 $r_2 < r_1 = \infty \text{ and } 1_{f(r,\theta)} = \begin{cases} 1 & \text{ if } f(r,\theta) > 0\\ 0 & \text{ if } f(r,\theta) = 0 \end{cases}$

•
$$CPD = \mu_2 - (\mu_1 - \mu_2) = 2\mu_2 - \mu_1$$

• $sCPD = \frac{\mu_2 - (\mu_1 - \mu_2)}{\sqrt{\varphi}} = \frac{2\mu_2 - \mu_1}{\sqrt{\varphi}}$

where
$$\mu_i = \frac{\int_{R_i} f(r,\theta) dA}{\int_{R_i} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_i} f(r,\theta) r dr d\theta}{\int_0^{2\pi} \int_0^{r_i} 1_{f(r,\theta)} r dr d\theta}, \quad \varphi = \frac{\int_{R_1} \{f(r,\theta) - \mu_1\}^2 dA}{\int_{R_1} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_1} \{f(r,\theta) - \mu_1\}^2 r dr d\theta}{\int_0^{2\pi} \int_0^{r_1} 1_{f(r,\theta)} r dr d\theta}, \quad i = 1, 2,$$

 $r_2 < r_1 = \infty \text{ and } 1_{f(r,\theta)} = \begin{cases} 1 & \text{ if } f(r,\theta) > 0\\ 0 & \text{ if } f(r,\theta) = 0 \end{cases}$

•
$$CPD = \mu_2 - (\mu_1 - \mu_2) = 2\mu_2 - \mu_1$$

• $sCPD = \frac{\mu_2 - (\mu_1 - \mu_2)}{\sqrt{\varphi}} = \frac{2\mu_2 - \mu_1}{\sqrt{\varphi}}$

where
$$\mu_i = \frac{\int_{R_i} f(r,\theta) dA}{\int_{R_i} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_i} f(r,\theta) r dr d\theta}{\int_0^{2\pi} \int_0^{r_i} 1_{f(r,\theta)} r dr d\theta}, \quad \varphi = \frac{\int_{R_1} \{f(r,\theta) - \mu_1\}^2 dA}{\int_{R_1} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_1} \{f(r,\theta) - \mu_1\}^2 r dr d\theta}{\int_0^{2\pi} \int_0^{r_1} 1_{f(r,\theta)} r dr d\theta}, \quad i = 1, 2,$$

 $r_2 < r_1 = \infty \text{ and } 1_{f(r,\theta)} = \begin{cases} 1 & \text{ if } f(r,\theta) > 0\\ 0 & \text{ if } f(r,\theta) = 0 \end{cases}$

 μ_1 : mean FA for entire brain

 μ_2 : mean FA for inner circle

•
$$CPD = \mu_2 - (\mu_1 - \mu_2) = 2\mu_2 - \mu_1$$

• $sCPD = \frac{\mu_2 - (\mu_1 - \mu_2)}{\sqrt{\varphi}} = \frac{2\mu_2 - \mu_1}{\sqrt{\varphi}}$

where
$$\mu_i = \frac{\int_{R_i} f(r,\theta) dA}{\int_{R_i} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_i} f(r,\theta) r dr d\theta}{\int_0^{2\pi} \int_0^{r_i} 1_{f(r,\theta)} r dr d\theta}, \quad \varphi = \frac{\int_{R_1}^{R_1} \{f(r,\theta) - \mu_1\}^2 dA}{\int_{R_1} 1_{f(r,\theta)} dA} = \frac{\int_0^{2\pi} \int_0^{r_1} \{f(r,\theta) - \mu_1\}^2 r dr d\theta}{\int_0^{2\pi} \int_0^{r_1} 1_{f(r,\theta)} r dr d\theta}, \quad i = 1, 2,$$

 $r_2 < r_1 = \infty \text{ and } 1_{f(r,\theta)} = \begin{cases} 1 & \text{ if } f(r,\theta) > 0\\ 0 & \text{ if } f(r,\theta) = 0 \end{cases}$

Convolutional Neural Network (CNN)

- Hierarchical layered representation learning
- A 2D representation via "back-propagation"

Credit: kaggle.com

Convolutional Neural Network (CNN)

- Find a set of values for the weights of all layers in a network associated with targets
- Adjust the value of the weights in direction of the lower cost (or loss) by an objective function, e.g., Binary Cross-Entropy

$$Loss = -\frac{1}{n} \sum_{1}^{n} \left\{ y_i \times \log(p(y_i)) + (1 - y_i) \times \log(p(y_i)) \right\}$$

Credit: Algendy 2020. Multi-Layer Perceptron (MLP)

Applying CPD to CNN architecture

- Recent work on imaging data
 - Application of CNN to automatic segmentation of breast lesion in Ultra Sound images (Costa et al., 2019)

Fig. 3 CNN2 architecture: first DAG architecture proposed for breast lesion segmentation in US image

Proposed CNN architecture

Figure 4. The proposed network architecture using CPD. The upper layers describe the CNN and the lower layers describe the MLP with 4 layers. The smaller the length of bar indicates the smaller size of the images. The number on top of each bar represents the number of nodes at the layer. The arrows with different colors represent different procedure as shown in the legend.

Proposed CNN architecture

- Key points of CNN+MLP with CPD
- 1. Adopt CNN: translation-invariant, spatial hierarchies for 2D images
- 2. Good features let you solve a problem with far less data
- 3. Training a **simple, well regularized** CNN model on a **very small data set** can potentially suffice and yield reasonable results
 - Simple: a small number of layers
 - Well-regularized: an optimized L2-norm λ value

- Introduction |.
- II. Methods
 - ✓ Concept of CPD
 - ✓ CNN+MLP architecture
- III. Results
- ✓ Applications to DTI studies: MagNeTS, ICBM IV. Discussion

Contents

Example DTI studies

- Study 1: Maryland MagNeTS prospective study from FITBIR
 - Traumatic Brain Injury (TBI) patients with baseline brain images
 - Access only DTI images (n=82) and estimate tensor information
- Study 2: International Consortium for Brain Mapping (ICBM) from LONI
 - Normal subjects' brain images for developing a MNI atlas template
 - Access only DTI images (n=192) and estimate tensor information

Training the model

- Input (X): DTI images and CPD
- Output (Y): Binary age group (Age ≤ 52 or > 52)
- Split data into training data and test data at ratio 80:20

Improved test accuracy on proposed model Results from MagNeTS data

Table 3. The models with best test accuracies for the CNN method alone and the CNN + MLP method using the MagNeTS data.

Model	Input	MLP	Radius	λ values	Training	Training	Test loss	Test
	data	design	r	$\left(\lambda_{_{mlp}},\lambda_{_{cnn}} ight)$	loss	accuracy		accuracy
CNN	Image			(NA, 3)	293.1302	0.7005	292.5994	0.6250
CNN+MLP	Image,	2 layers	5	(0.01, 0.5)	51.3255	0.6973	51.5627	0.7083
	unscaled		15	(0.1, 0.5)	52.6860	0.7582	51.3741	0.7083
	CPDs		5, 15	(0.01, 0.5)	51.3449	0.7659	50.8401	0.7083
		4 lavers	5	(1, 0.5)	70.7909	0.7183	70.9441	0.7083
			15	(0.1, 0.5)	53.2396	0.7872	52.6477	0.7500
			5, 15	(0.01, 0.5)	52.0297	0.8125	51.9336	0.7500
	Imaga	2 lovora	5	(1, 0, 5)	07194	0 7414	0 7625	0 7082
	mage,	2 layers	5	(1, 0.5)	0.7104	0.7414	0.7023	0.7083
	scaled		15	(0.05, 0.5)	0.8342	0.7586	0.8405	0.7083
	CPDs		5, 15	(0.1, 0.5)	1.6615	0.7241	1.6553	0.7500
		4 layers	5	(0.01, 0.5)	1.4807	0.7414	1.5009	0.7083
		•	15	(1,0.5)	1.4562	0.7414	1.4908	0.7083
			5, 15	(0.1, 0.5)	2.4740	0.7069	2.4500	0.7500

Improved test accuracy on proposed model Results from ICBM data

Table 5. The models with best test accuracies for the CNN method alone and the CNN + MLP method using the ICBM data. We train the CNN + MLP model with both CPD₅ and CPD₁₅. Complete data rate indicates the threshold percentage of available FA values inside the basis circle from the center image. For example, 70% indicates the images where 70% or greater of FA values are available inside circles at both radii.

Model	Input data	Complete data rate	$\lambda \text{ values} \ \left(\lambda_{mlp},\lambda_{cnn} ight)$	Training loss	Training accuracy	Test loss	Test accuracy
CNN	Image		(NA, 0.1)	11.3143	0.7188	12.3710	0.6379
CNN+MLP	Image, unscaled CPDs	70% No restriction	(3, 0.1) (0.1, 0.1)	56.6895 13.1572	0.7031 0.6493	56.7059 15.6420	0.6897 0.6379
	Image, scaled CPDs	70% No restriction	(3,0.1) (0.01,0.1)	50.2584 11.2429	0.7031 0.7463	49.8063 12.4016	0.6897 0.6724

- Introduction Ι.
- II. Methods
 - ✓ Concept of CPD
 - ✓ CNN+MLP architecture
- III. Results
 - ✓ Applications to DTI studies: MagNeTS, ICBM
- IV. Discussion

Contents

New paradigm for DTI study

Our consideration of algebraic variants for brain's characteristic may complement information not revealed through CNN's feature selection

New paradigm for DTI study

Our consideration of algebraic variants for brain's characteristic may complement information not revealed through CNN's feature selection

Advantages

- A. No experts' opinion to search for regio
- B. CPD may not require very crisp images
- C. CPD may complement information not revealed by CNN's feature selection

		Disadvantages
ons	A.	Need more physiologically relevant representation
S	B.	Data size is not enough for generalization

New paradigm for DTI study

- Future work
 - 1. Extend it to multi-centric peripheral deviation
 - 2. Apply it to 3D in order to verify justification of 2D approach
 - 3. Find the best criteria for λ change in each layer
 - 4. Use other diffusion coefficients such as Mean Diffusivity, Radial Diffusivity, Axial Diffusivity

